

## New Frontiers: Medical Aerosols in Critical Care

Jim Fink, RRT, PhD, FAARC, FCCP Independent Consultant Adjunct Professor, GA State University and Rush Medical School, Chicago Fink.jim@gmail.com

Suncoast Symposium

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# **Disclosures**

## Scientific advisory board , Chief Clinical Officer

• Aerogen, ireland

## Consultant

- Aerogen
- Ansun
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- Bayer
- Boerhinger Ingleheim
- Dance Biopharm
- Parion
- Quark
- WHO

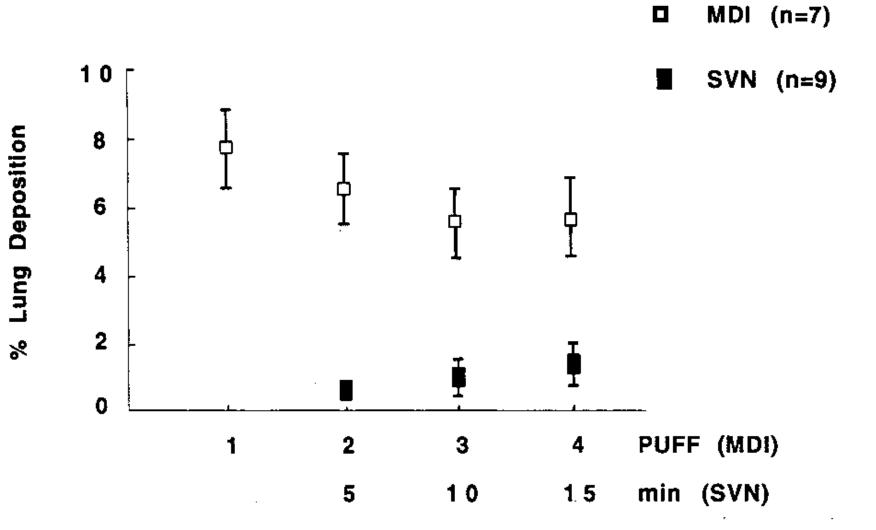
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# **Types of Ventilators : Invasive and Noninvasive**



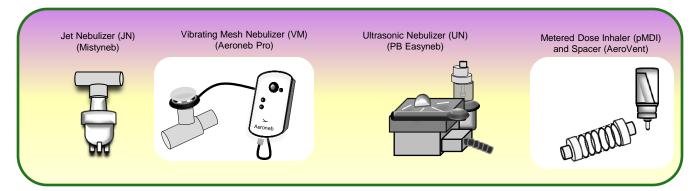
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				bated jects	Nonint Subj		
	Administered radi Percent of adminis dioactivity in:	+	5.75 ±	1.3 mCi	6.53 ± 0	).4 mCi	-
	Trachea (includ of endotrache intubated pati	al tube in	1.6 ±	1.1%"	0.3 ± 0	0.1% <sup>a</sup>	
	Lung parenchyr	na	$2.9 \pm$	0.7% <sup>b</sup>	$11.9 \pm 2$		
	Stomach		-	_	$7.3 \pm 2$		
	Oral cavity		-	_	$15.0 \pm 1$		
	Nebulizer circui	try	-	_	65.5 ± 1	6%	

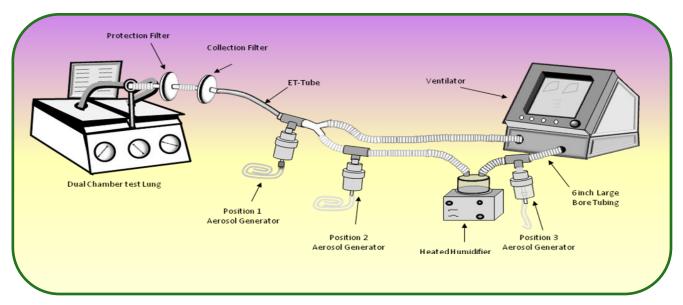
Macintyre Crit Cre Med 1985



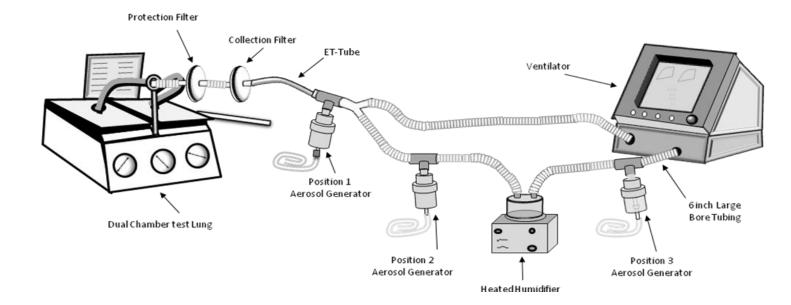
Fuller et al. 1990. ARRD 141:440-444.

# Four types of aerosol generators in 3 positions during CMV with no bias flow



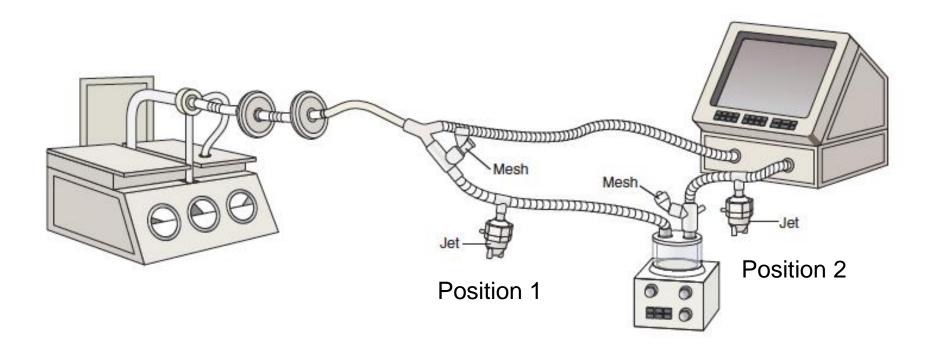


Ari et al. Respiratory Care 2010; 55 (7): 837-844.

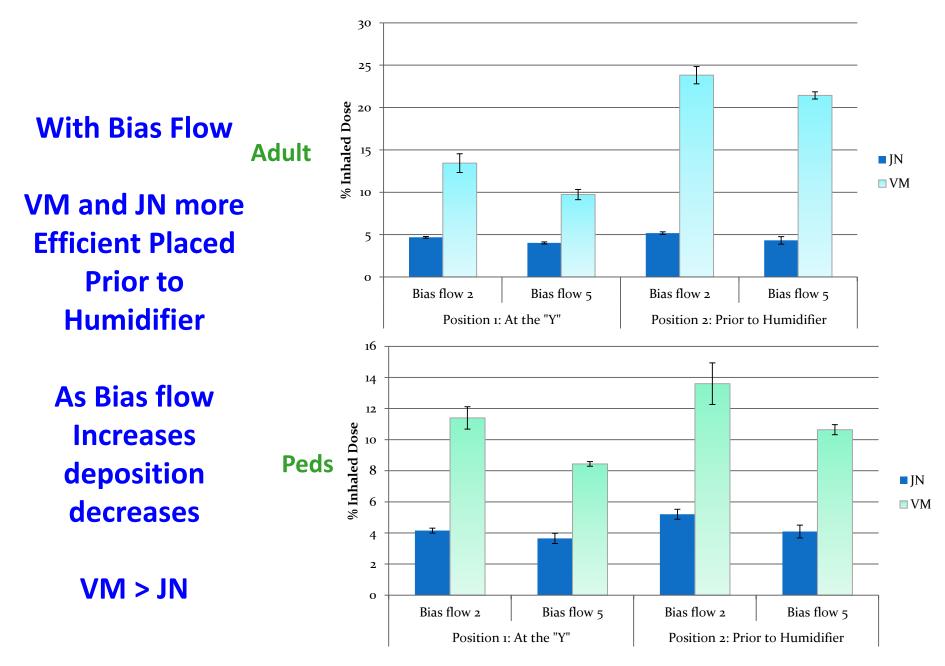


Neb Position	Pos 1 - Between ETT & Y		Pos 2 - 6 in from Y		Pos 3 - 6 ii	n from Vent
Ventilator Circuit	Heated	Unheated	Heated Unheated		Heated	Unheated
JN	4.66 (0.5)	7.62 (0.9)	3.61 (0.2)	9.66 (1.5)	5.98 (0.1)	14.66 (1.5)
VM	12.82 (0.5)	14.54 (1.0)	16.79 (2.6)	30.24 (1.0)	8.39 (2.1)	24.20 (1.2)
UN	10.07 (3.9)	10.70 (1.5)	16.53 (4.3)	24.68 (4.4)	4.59 (2.0)	10.51 (0.3)
pMDI	7.6 (1.3)	22.1 (1.5)	<b>17 (1.0) 27.8 (3.3)</b>		2.5 (0.8)	7.9 (1.5)

Ari et al, Respir Care 2010



	ADULT STUDY	PEDIATRIC STUDY	
Mode	Volume Control	Volume Control	
Tidal Volume	500 ml	100 ml	
Respiratory Rate	20/min	20/min	
PEEP	5 cmH <sub>2</sub> O	5 cmH <sub>2</sub> 0	
Waveform	Descending	Descending	
Bias Flow	2 and 5 lpm	2 and 5 lpm	
Ari et al. Res	oiratory Care 2010; 55 (7)	: 845-851.	

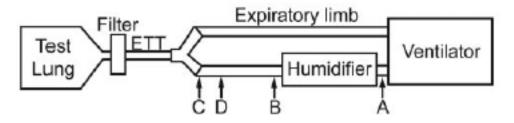


Ari et al. Respiratory Care 2010; 55 (7): 845-851.

## **4 Nebulizers in 4 Positions of Pediatric Vent**



Fig. 1. Nebulizers tested. From right to left: Aerogen Solo, Maquet Ultrasonic model N06302595E400E, Salter 8900, and Hudson Updraft II Opti-Neb.

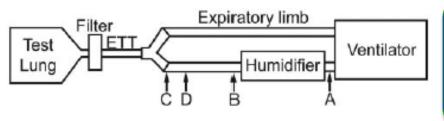


Pressure Regulated Volume Control. Vt 200 mL, Rate 20 bpm, PEEP 5,  $T_{insp}$  0.75 s, bias flow 2L/min, 37 degree C

Berlinski A and Willis JR. 2013 Respir Care

# Bench study: Nebulizer position determines nebulizer performance

Albuterol Loading	Nebulizer	Nebulizer position					
volume		At Ventilator	At Humidifier	At Y-piece	30cm Before Y- piece		
2.5mg/ 3ml	Hudson Updraft II Opti-Neb	$5.4 \pm 0.6$	$4.7 \pm 0.8$	$2.0 \pm 0.1$	$4.3 \pm 0.8$		
	Salter 8900	$3.1 \pm 0.9$	4.6 ± 0.9	$2.8 \pm 0.4$	$2.9 \pm 0.7$		
	Maquet Ultrasonic	12.8 ±1.5	17.1 ± 1.5	8.7 ± 0.7	10.5 ± 2		
	Aeroneb Solo	$28.5 \pm 8.6$	33.3 ± 3.6	8.7 ± 2.5	$10.3 \pm 3.3$		

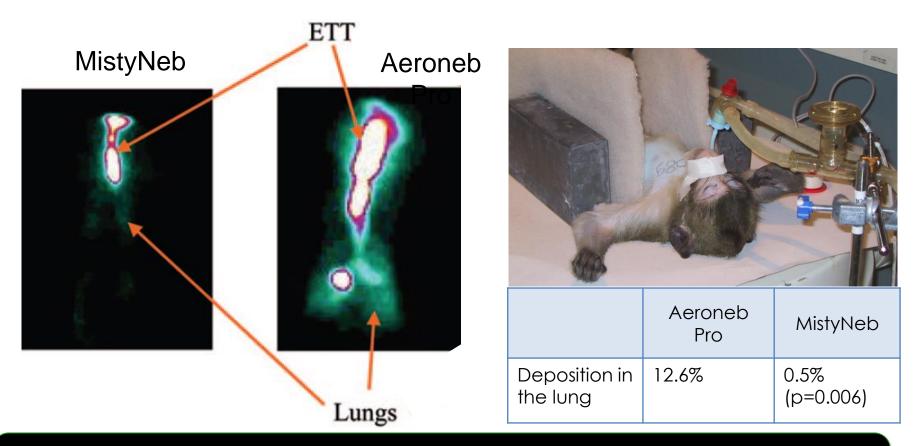


Bias Flow 2L/min

The Aeroneb Solo performance was 5-6 times superior to small volume nebulizers ad outperformed all others at all locations.

Berlinski & Willis, 2013.

# Vibrating Mesh - Drug Deposition in animal model of infant ventilation



## ~25-fold greater lung deposition with Aeroneb Pro compared to a Jet nebulizer during infant ventilation

Dubus et al. 2005 Aerosol deposition in neonatal ventilation

#### ILOPROST DRUG DELIVERY DURING INFANT MECHANICAL VENTILATION: INFLUENCE OF NEBULIZER POSITION DURING CONVENTIONAL AND HIGH FREQUENCY VENTILATION

HYPOTHESIS

We designed studies in who to test the hypothesis that there were no differences in drug delivery between conventional and HFOV, testing two

Robert M DiBlasi RRT-NPS FAARC,<sup>1,2</sup> Shuijie Shen PhD,<sup>1</sup> David N Crotwell RRT-NPS FAARC,<sup>2</sup> John Salyer RRT-NPS FAARC,<sup>2</sup> Delphine Yung MD<sup>1,3</sup>

<sup>1</sup> Center for Developmental Therapeutics, Seattle Children's Research Institute, Seattle WA, United States

<sup>2</sup> Respiratory Therapy Department, Seattle Children's Research Institute, Seattle WA. United States

<sup>3</sup> University of Washington School of Medicine, Seattle WA, United States

\* This study was funded through a grant provided by CDT at SCRI and drug was provided by Actelion

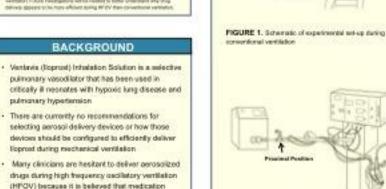
#### ORIGINAL ABSTRACT

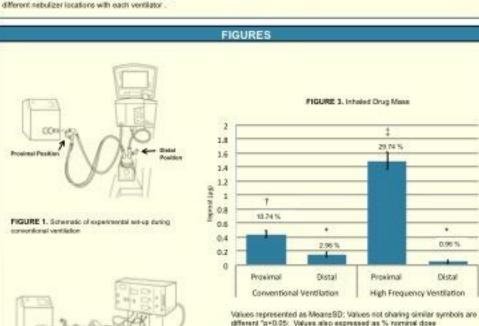
infants with simple large distance (CLE), community separat postorped manalers ambalancedending layout the CU. NTRODUCTION Venaulo (historia) initialation Solution is a selective polynomial viscolitate that to const-orky sead or othody Encontrast with hyperin Juny domain and puttionary hyperbension. The Peakered-AADR System is the unit FDN asymptotic defines for Appoint has this redulate turned its used its inte during minimumat variation. There are mananity to telephoneniations for aslanting senses stilling devices to how forest similars should be carriented to effectedly deliver Septemblizing reachering weldator: Monover: mana calificiana are feature to deliver top-bit during high traggeney contracts validation prifting bacausa in a balaved that madication latively & englights due to furture on and tidal rotures, will high bits free-will this fam of rendshan the designed studies in vitia to led the hypothesis that have water the differences in data delivery between two different tetration treations during contentional and HPOY, METHOD & 3 naturated and lang model (ARL 1000, Higher Method and configured atte C. 1.8 millionPAG and PLID ant AGEs. The Key. instel was tentioned after a tendeninetal randiativ and WOV with standard ethigs and have distant device DRYCs. Highlan 20 mics was hetwised using The Amonato Pro (Amongeo, 19-3) photos (Contenue) the partners and the ET Life. (Polympi) and the vertilated and insmitter (Solar). Uses prevents were obtained in trainate airs from different tabalants in such of its send tarations. Report that was surveyed by along the like with attanci and quantitati away high processes Input streaman graphy Differences instances must strep trate same companed at each condition calleg MIENN with Tubey post-loci tubes. Significance was normalist av pret. IN, REPAR'S conter pl sading conditions, graner plug delivery was advanced with the reduktion placed to be Pleaster poption than the State position during conventioned and 4P/OV (p-2.30). There east teer's 8 3-634 grouter increase indicat defeaty during NPDV that increasing an indicator Physics. DESCUBBIOM/DOM/DUMBIOME improve shop delivery in teast antisened strum-the restrictives in placest interest time IT take and patient area during manhanital settistory if ours resultations white needed to belter understand why drug perved appears to be more efficient sining thi dV than convertision vertil

delivery is negligible due to the small volumes, short

inspiratory times and high gas flows used with this

form of ventilation





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 An ASL 5000 (ingmar Medical) configured with compliance: 1.0 mL/cmH\_D and resistance: 50 cmit, D/Lis was vertilated with a conventional ventilator and HFOV with standard settings and heated humidification (39°C) connected to a 3.5 ID ET-tube (FIG: 1 and 2)

METHODS

Seattle Children's

- The Aeroneb Pro8 (Aeronen, Galeway, Ireland) was tested in two different locations: 1) between the humidifier probe and patient wye (Proximal) and 25 between the ventilator and humidifier (Distal)
- lipprost (30 mog) was nebulized in three trials with nere rebuiltoirs (n=3) in each of the dirout locations. Reprost was recovered from a filter by eluting the filter with othanol and guantified using high pressure liquid chromatography
- Differences between mean drug mass were compared at each condition using ANOVA with Tukey post-hoc tests. Significance was determined as p+0.05

#### RESULTS

- During conventional and HEOV, drug delivery was greater with the nebulizer placed in the proximal position compared to the distal position (p=0.05)
- There was nearly a 3-fold greater increase in drug. delivery during HFOV than convertional ventilation is the Proximal position (FIG. 3, p40.05)

#### DISCUSSION/CONCLUSION

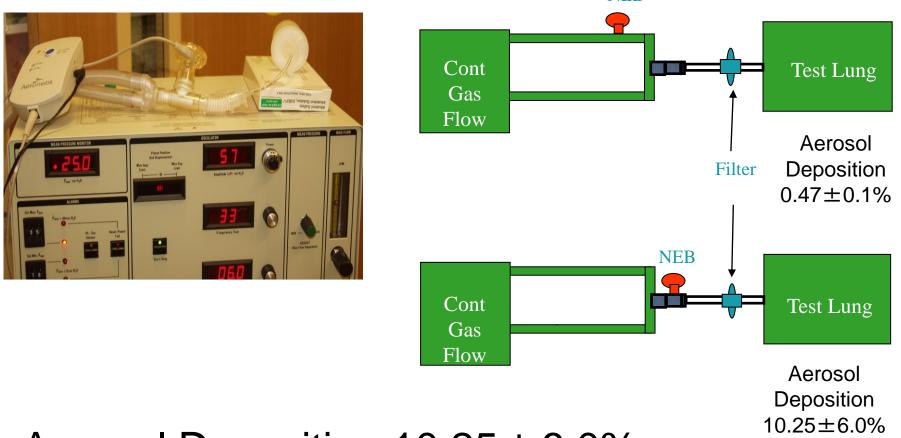
- Boprost drug delivery is best achieved when the nebulizer is placed proximal to the patient-www.during neoratal mechanical ventilation
- Puture investigations will be readed to better understand why drug delivery appears to be more efficient during HFOV than conventional ventilation.

FIGURE 2. Schomaliz of Experimental Sel-ap during highfrequency asplitatory ventilation



# For HFOV: Place Neb between circuit and ETT

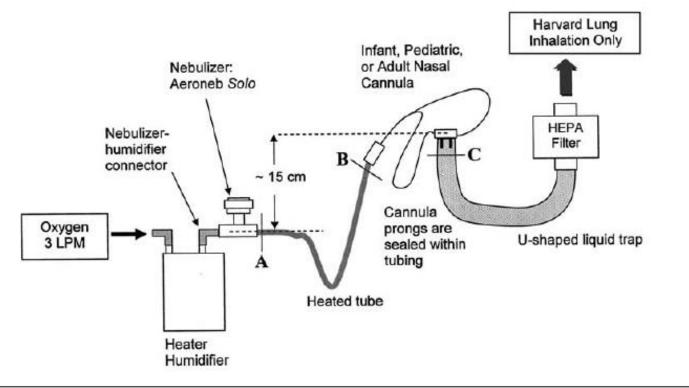
**NEB** 



# Aerosol Deposition $10.25 \pm 6.0\%$

Demers et al. ATS San Diego, 2005

## **Aerosol Delivery via Nasal Cannula**



	Infant cannula		Pediatric cannula		Adult cannula	
	No Harvard lung	Harvard lung	No Harvard lung	Harvard lung	No Harvard lung	Harvard lung
Aerosol output dose (%) delivery time (min)	8.4 ± 2.3 13.1 ± 2.5	$18.6 \pm 4.0$ $10.8 \pm 0.7$	$18.1 \pm 4.2$ $13.0 \pm 0.0$	$25.4 \pm 1.7$ $10.9 \pm 1.4$	$25.1 \pm 5.0$ $12.5 \pm 0.4$	$26.9 \pm 4.9$ $12.1 \pm 0.8$

### Bhashyam et al. JAM 2008

## **Aerosol Delivery via Nasal Cannula**

	Infant cannula		Pediatric cannula		Adult cannula	
	No Harvard lung	Harvard lung	No Harvard lung	Harvard lung	No Harvard lung	Harvard lung
Losses in cannulas Losses in nebulizer Losses in nebulizer– humidifier connectors	$3.5 \pm 2.0$ $2.2 \pm 0.3$ $25.6 \pm 5.9$	$7.5 \pm 1.1$ $3.4 \pm 0.6$ $20.4 \pm 17.7$	$7.8 \pm 5.2$ $3.5 \pm 1.1$ $27.8 \pm 12.7$	$6.6 \pm 3.1$ 2.7 ± 0.8 17.3 ± 11.9	$12.3 \pm 5.0$ $2.8 \pm 1.4$ $26.0 \pm 16.2$	$10.8 \pm 2.9$ $2.4 \pm 0.6$ $20.7 \pm 8.2$
Losses in heated tube Losses in U-shaped liquid trap	$30.7 \pm 4.3$ $3.0 \pm 3.8$	$32.1 \pm 7.8$ $1.0 \pm 1.0$	37.3 ± 2.5 3.8 ± 3.0	$35.0 \pm 11.6$ $1.8 \pm 0.5$	$27.1 \pm 1.7$ $1.1 \pm 0.4$	28.5 ± 2.5 2.1 ± 1.5
Losses in heater/ humidifier (assumed)	26.7 ± 3.7	$17.1 \pm 8.8$	$1.7 \pm 1.1$	$11.1 \pm 5.4$	$5.6 \pm 11.8$	8.7 ± 5.8

TABLE 2. SUMMARY OF COMPONENT LOSSES FOR THE NASAL CANNULA AEROSOL DELIVERY SYSTEM SHOWN IN FIGURE 1

TABLE 3. AEROSOL SIZE MEASUREMENTS AT DIFFERENT POINTS IN THE NASAL CANNULA AEROSOL DELIVERY SYSTEM

Meas. point		$VMD \ \mu m$	Dv90 µm
A	Exit of nebulizer	$5.0 \pm 0.2^{*,**} \\ 4.2 \pm 0.7^{*,**} \\ 2.2 \pm 0.2^{*,,***} \\ 1.9 \pm 0.3^{**,***} \\ NM$	$8.9 \pm 0.8$
B	Exit of heater tubing		$6.8 \pm 1.5$
C	Adult cannula		$4.2 \pm 0.4$
C	Pediatric cannula		$3.8 \pm 0.5$
C	Infant cannula		NM

### Bhashyam et al. JAM 2008

# Aerosol Delivery with High Flow Nasal Cannula with Adult Cannula

	10 lpm	30 lpm	50 lpm
02	27.1%	12.03%	3.6%
80%Heliox	27.9%	14.4%	5.6%

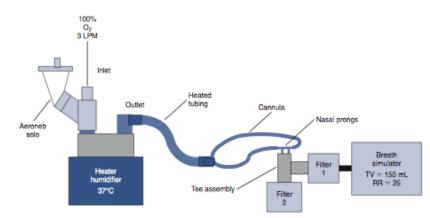


FIGURE 4-44 In vitro setup for testing aerosol delivery with a heated humidifier through a nasal cannula. The nebulizer is placed at the inlet of the humidifier, and the cannula is attached to a T-piece that allows aerosol to collect on filter 1 and condensate to collect on filter 2. This device can be used in infants, children, and adults.

Ari, Dailey, Fink 2009

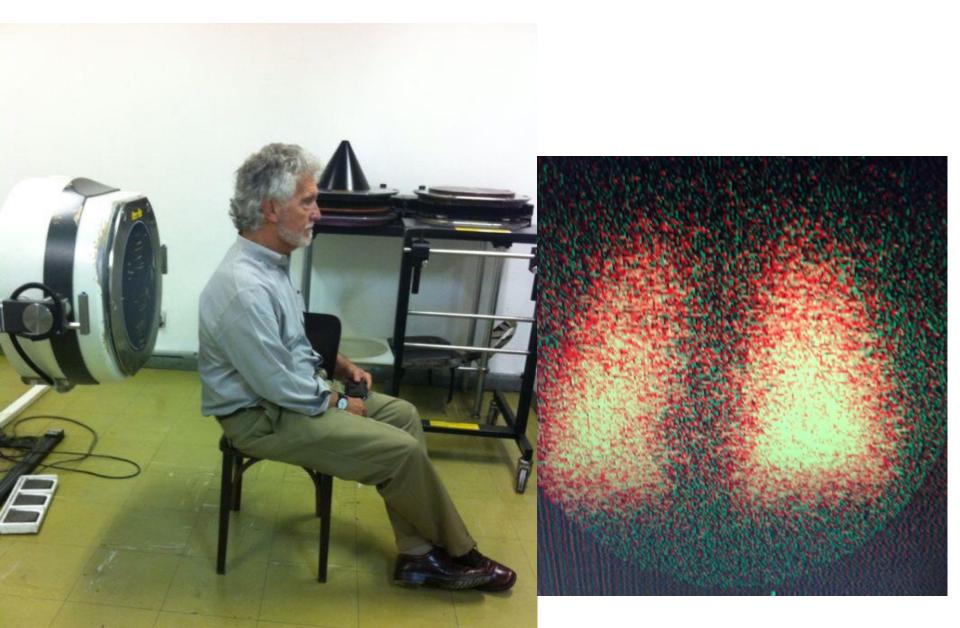
## **High Flow Nasal Cannula**



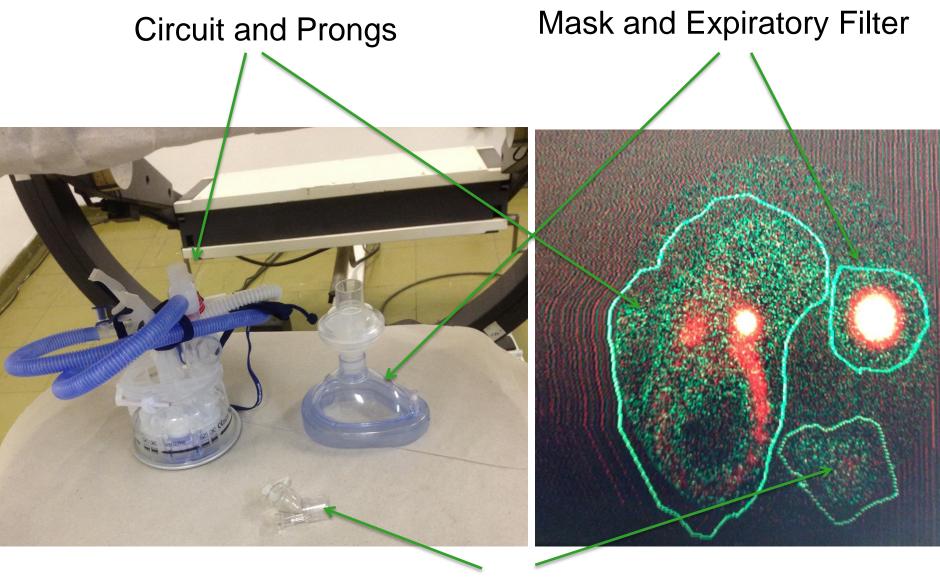
# Mask with filter placed over the nasal cannula to collect aerosol that is not inhaled and aerosol that is exhaled.



After administration, anterior scan of thorax for 300 secs with a 256x256 matrix.

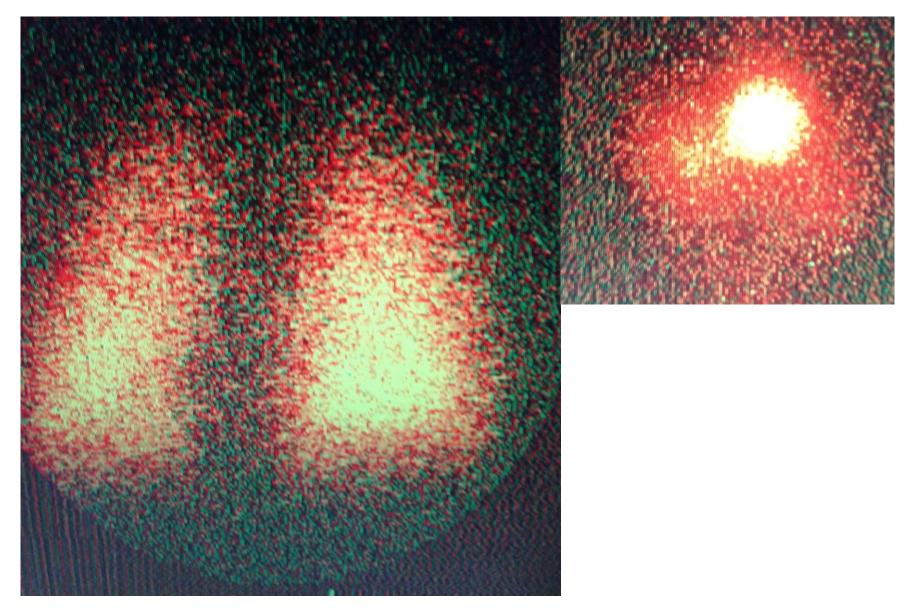


Circuit and nasal prongs, Mask with filter, nebulizer scanned.



## Nebulizer

# HFNC 10 L/min 1 mCi in 1 mL



### Study of Deposition with HFNC in an adult using two radiation doses 1 mL total dose with Vibrating Mesh nebulizer with 10 L/min Oxygen

			HFNC 10 lpm 1 mCi				1/2 mCi
Left Lung	73136		1 mei	Left Lung	36962		1/2 11101
Right lung	87462			Right lung	46972		
Lung total	160598		15.4%	Lung total	83934		15.6%
stomach	2371		0.2%	stomach	1351		0.3%
Head	82133		7.9%	Head	47761		8.9%
Inhaled		245102	23.4%	Inhaled		133046	24.8%
Neb	15496		1.5%	Neb	9600		1.9%
circuit	277622		26.5%	circuit	163141		32.3%
Filter	347085		33.2%	Filter	115468		22.9%
		706840	61.2%			279569	57.0%

### Total Count 1045903

Total Count 505189

# **Observations Conclusion**

## N=2 feasibility study in an adult subject

## Consistent results with both 1 and 0.5 mCi

Future studies should be with the lower inhaled dose, and determine lower limits

## • 23 – 24% inhaled dose

Consistent with previous in vitro models

## 15% lung dose

Very low stomach deposition

Homogenous distribution through lungs

#### Ergonomic and High Efficiency Trans-Nasal Aerosol Delivery Platform Targeting Pulmonary Deposition with Minimal Deposition in the Nose

T Navratil<sup>1</sup>, KL Zeman<sup>2</sup>, F Fuller<sup>2</sup>, D Taylor<sup>3</sup>, W Thelin<sup>1</sup>, P Boucher<sup>1</sup>, B Button<sup>2</sup>, J Fink<sup>4</sup>, AJ Hickey<sup>5</sup>,

RC Boucher<sup>2</sup>, MR Johnson<sup>1</sup>, S Donaldson<sup>2</sup>, WD Bennett<sup>2</sup>

 Parion Sciences, Inc., Durham, NC, United States; 2. University of North Carolina, Chapel Hill, NC, United States; 3. Cambridge Consultants, Cambridge, United Kingdom; 4. Georgia State University, Atlanta, GA, United States; 5. RTI International, Research Triangle Park, NC, United States.

#### Background

- Trans-nasal delivery of aerosols to the lungs may offer benefits over the oral route for a range of patient populations and healthcare settings
- In supplemental oxygen studies, patients favor ergonomic nasal cannulas over face masks
- However, aerosols from conventional nebulizers are not suitable for delivery via narrow-bore nasal cannulas (large particles > 4 μm impact or sediment during the travel through the nasal cannula)
- The reported pulmonary deposition efficiencies of trans-nasal aerosols in human subjects have been low (approximately 1-5% of the emitted dose)
- Parion's Trans-nasal Pulmonary Aerosol Delivery (tPAD) platform aims to enable delivery of aerosols via an ergonomic, optimized supplemental oxygenlike nasal cannula over extended periods of time with deposition efficiencies equaling that of oral aerosol delivery

#### Objectives

- To design and develop a Trans-Nasal Pulmonary Aerosol Delivery device (tPAD device) for use with hyperosmotic agents, antibiotics, mucolytics and other agents for extended administration towards (1) accommodating patient preferences; (2) improving efficacy and tolerability of these agents; and (3) reducing daytime treatment burden in CF and other respiratory diseases
- ◆ To determine safety, tolerability and deposition efficiency of the tPAD device in a Phase 1 clinical study in healthy human subjects



#### Patient Preferences for the tPAD Device

- A Human Factors Study was conducted to determine patient preferences for a concept trans-nasal aerosol delivery device were determined in interviews with 31 CF patients
- The conceptual tPAD platform was presented as an overnight aerosol delivery device to replace daytime inhaled CF medications

#### Table 1. Select Demographic and Inhaled Pharmacotherapy Data for CF Patients in Human Factor Study (Median of 2.5 h of Pharmacotherapy/Day)

Key Traits	Age			Concomitant Medications				
Indits	5-12	5-12 13-17 18+ DNase HS Tobramycin		Cayston	ľ			
% (n)	26% (8)	26% (8)	48% (15)	97% (30)	77% (24)	45% (14)	42% (13)	

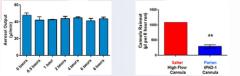
#### STUDY RESULTS:

- 90% of CF patients spontaneously indicated they would use tPAD platform
  Most suggested to deliver all inhaled therapy in tPAD
- Supplemental oxygen cannula was preferred to CPAP or other face-piece device



#### from the Nasal Cannula over 8h

than High Flow Oxygen Cannulas

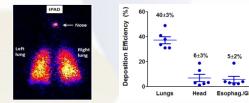


#### tPAD-1 Deposition Study in Healthy Volunteers

 Parion conducted a Phase 1 Safety, Tolerability and Deposition Efficiency Study of Radio-Labeled 7% Hypertonic Saline (%) TC-DPTA) Administered by the tPAD-1 Device to Healthy Human Subjects in collaboration with the University of North Carolina at Chapel Hill

#### STUDY RESULTS:

- In 6 healthy human subjects (3 males, 3 females; age >18 years), there were no adverse events, intolerability events, or measurable decreases in FEV<sub>1</sub> as detected in safety spirometry
- The tPAD-1 Device demonstrated substantially higher pulmonary deposition (and lower nasal deposition) compared to traditional nasal aerosol delivery techniques)



Representative gamma-camera scan following 15-min administration of <sup>99m</sup>Tclabeled 7% hypertonic saline by the tPAD-1

#### Conclusions

Regional deposition efficiencies for 7%

hypertonic saline administered by the tPAD-1

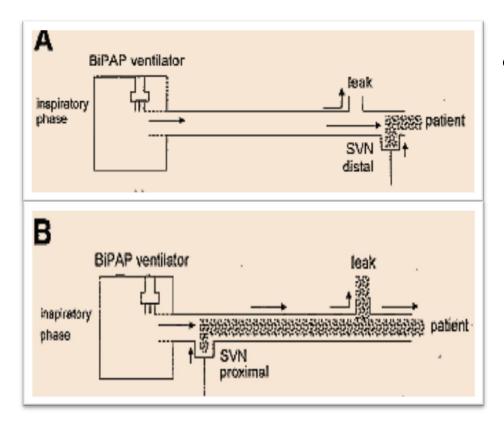
Device (Mean ± SEM)

- High level of patients' willingness (28/31) to adopt the tPAD platform was identified in a human factor study preceding the tPAD device development
- tRAD-1 Devices produces consistent aerosol output, controlled aerosol particle size ~1.4 µm VMD, and very limited "sputter" from the prongs of nasal cannula were achieved
- Excellent safety, tolerability and high pulmonary deposition efficiency (38% based on emitted dose) were demonstrated with the tPAD-1 device in healthy human subjects in Phase 1 clinical study
- Parion Sciences is developing the tPAD platform in combination with hydrating agents to improve the efficacy and tolerability of these agents and to reduce the daytime treatment burden in CF and other respiratory diseases

Studies Funded by Parion Sciences and NIH Grant 1 PO1 HL 108801-01A1

#### tPAD Device Performance

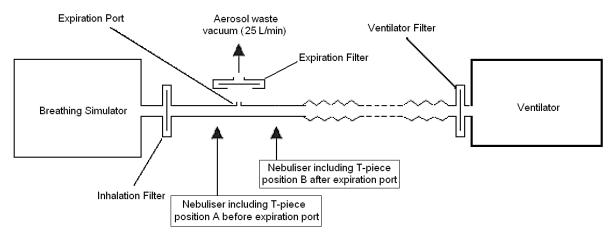
# Aerosol Delivery and NIV – place neb between leak and patient



- Drug delivery influenced by:
  - Nebulizer position
  - Breathing frequency
  - IPAP/EPAP settings

Chatmongkolchart S et al Crit Care Med 2002;30:2515-2519.

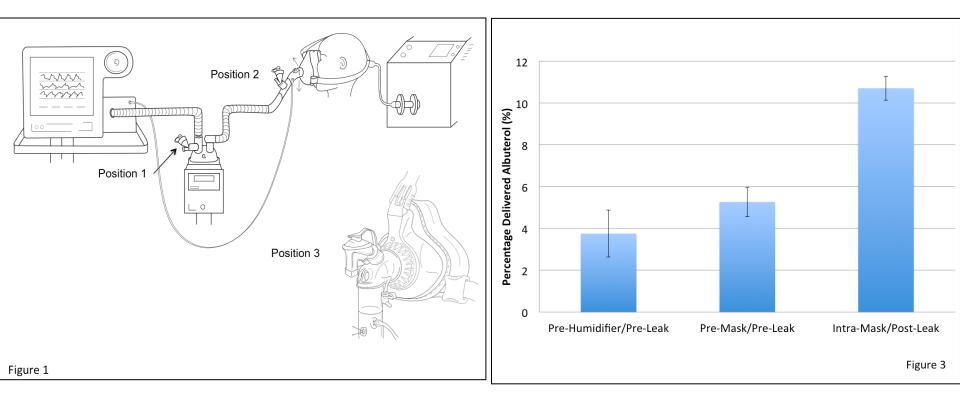
## **Position Neb Between Leak and Mask for best delivery**



Nebulizer	Position closer to filter (A)		bulizer Position closer to filter (A) Positi			rom filter (B)
	Inhalation Filter (µg) (µg)		Inhalation Filter (µg)	Nebulizer (µg)		
Aeroneb	2573	891	936	1001		
	± 151	±163	± 273	± 263		
Sidestream	1207	2261	341	2420		
	± 161	± 795	<b>±</b> 70	± 154		

Abdelrahim ME et al J Pharmac Pharmacol 2010; 62;966-72.

## Bench Study: Pediatric aerosol delivery during noninvasive ventilation with the NIVO



# Comparison of aerosol delivery with the NIVO and the Aeroneb Solo during non-invasive ventilation

White CC, 2013. Bronchodilator delivery during simulated pediatric noninvasive ventilation. Respiratory Care. Published ahead of print February 5, 2013, doi:10.4187/respcare.02171

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#### EFFICIENCY OF AEROSOL DEVICES DURING NONINVASIVE POSITIVE PRESSURE VENTILATION IN A SIMULATED ADULT LUNG MODEL

Maher M. AlQuaimi BsRc RRT, James Fink PhD, RRT, FAARC, FCCP, Robert Harwood, MSA, RRT, Meryl M Sheard MSc RPFT, Arzu Ari, PhD, RRT, PT, CPFT, FAARC Georgia State University, Atlanta, GA

Experimental setup used with VMN, JN, and pMDI

Test Lung

Bilevel Ventilator					
Bilevel Ventilator					
		JN	VMN	pMDI-N	pMDI-R
Collecting Filter	Inhaled Mass (mg)	0.33 ± 0.02	0.72 ± 0.05	0.10 ± 0.01	0.09 ± 0.01
	Inhaled Mass Percent (%)	13.12 ± 0.72	28.83 ± 1.93	23.53 ± 2.03	21.38 ± 0.32
Leak Port	Residual volume (ml)	1.65 ± 0.14	0.10 ± 0.07		
Collecting Filter	Vibrating Jet	Mesh (V	MN) > 2	fold more	e than
Leak Port	VMN and	pMDI sii	milar dos	se efficie	ncy
Collecting Filter	3				

# Lung Dose JN vs Mesh



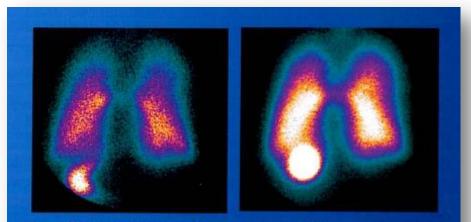


Figure 2: Typical distribution of aerosol deposited in lungs with JET(left) and MESH (right) with 3 mL dose volume.



Lung deposition (corrected for absorption) with the Mesh was > 3 fold greater than JN, independent of dose volume used with the MESH.

Neb/Dose	JET NEB 3 mL	MESH 3 mL
Total Lungs	1.97 ± 0.8%	8.26 ± 1.1 %*
Inhaled Dose	7.31 ± 4.3%	27.3 ± 10.1 %*

\*p<0.0001 (MESH 3 mL vs JN 3 mL) and \*\*p<0.007 (MESH 1 mL vs JN 3 mL).

## **Medications via Aerosol to Intubated Patients**

- Bronchodilators
- Anti-infectives
- Prostanoids
- Anticoagulants Heparin
- Diuretics
- Insulin
- Perfluorocarbons (PFCs)

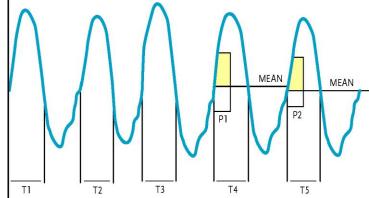
# Limitations to Delivery of Prostacyclincs in the ICU/OR

 Iloprost and Treprostinil are only drugs approved for treatment pulmonary hypertension for inhalation in adults, but not readily available for use in the ICU

## Flolan is not approved for inhalation

- Has short half life 2 3 minutes, requiring continuous aerosol delivery
- In general it is better to use drugs approved for inhalation when they are available.
- Difficult to translate between devices to determine comparable dosing.

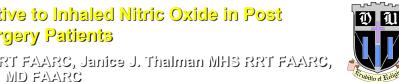






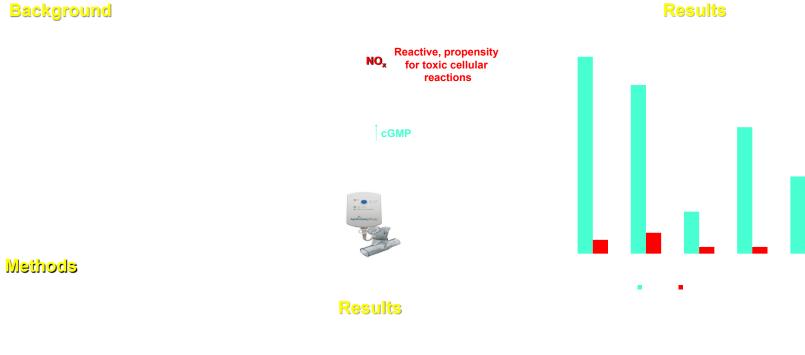




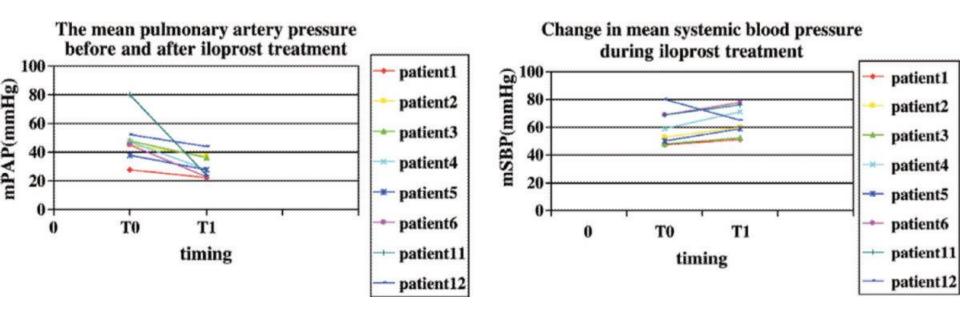


#### Aerosolized Iloprost is a Viable Alternative to Inhaled Nitric Oxide in Post Cardiothoracic Surgery Patients

John D. Davies MA RRT FAARC, Michael A. Gentile RRT FAARC, Janice J. Thalman MHS RRT FAARC, Neil R. MacIntyre MD FAARC Duke University Medical Center Durham, NC

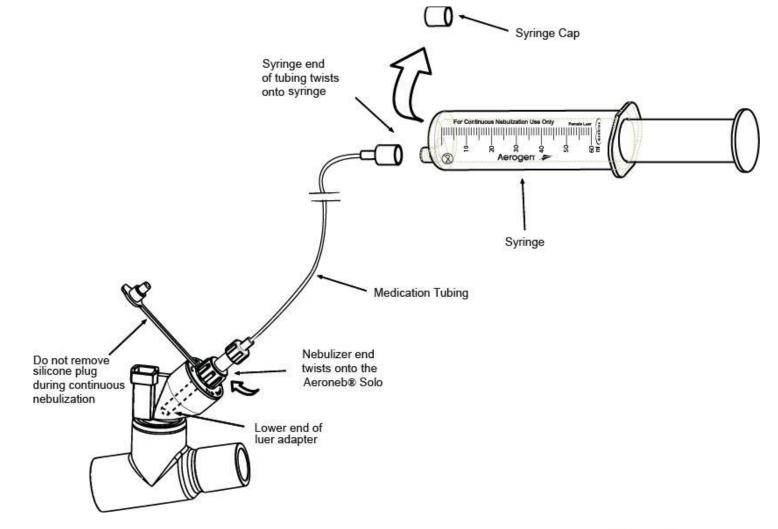


Conclusion



Effect of inhaled iloprost in 12 children with postoperative congenital heart disease. Iloprost lowered mean pulmonary artery pressure (mPAP) without lowering mean systemic blood pressure (mSBP). Limsuwan et al

# **Continuous Feed Set**





# **The Pulmonary Infusion Pump**

- A precise variable aerosol delivery system
- Medication is nebulized " drop by drop " as it reaches the aerosol generator
- Aerosol is not generated between drops
- For continuous aerosol therapy Mesh is on continuously, and aerosol is generated intermittently
- Pump rate is directly linear with aerosol output rate.
- No buildup of acerosl in reservoir.



## Conversion from inhaled nitric oxide to inhaled epoprostenol reduces costs of inhaled pulmonary vasodilator therapy in critically ill patients

Su san LaGambin a RRT1, Paul Nuccio MS RRT FAARC1, Heather Torbic PharmD BCPS2 Kevin E, Anger PharmD BCPS2 Paul M, Szumita PharmD BCPS2 Gerald Weinhouse MD3

Department of Respiratory Care Services1; Department of Pharmacy? Pulmonary Division 3, Brigham and Women's Hospital, Boston, MA

Patient Errollment

e analyzi

2 pill lents

#### Background

- Inhaled nitric oxide (iNO) and inhaled epoprostenol (iEPO) are potent pulmonary vasodilators that have been given off label as rescue therapy for severely hypoxic, critically ill patients
- Limited data exists evaluating the efficacy of these agents in a diverse cohort of critically ill patients

#### Purpose

To des cribe process and associated costs for inhaled epoprostenol use

#### Methods

- Retrospective, single-center analysis of adult mechanically ventilated (MV) patients receiving iNO or iEPO for pulmonary vasodilation
- Patients were enrolled between January 1, 2009 and October 31, 2010
- This study was approved by our institutional IRB
- Inclusion criteria
- > 18 years old
- Admitted to an intensive care unit at Brigham and Women's Hospital
- Received either iNO or iEPO

Exclusion criteria

 Received > 2 hours of concornitant iNO and iEPO

ata	assessed

Patient demographics

Methods

- Therapy duration
- · Cost

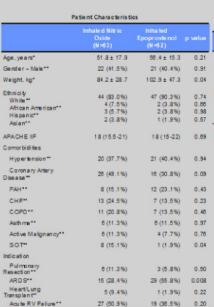
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#### Outcomes

- Cost
  - Total cost of iNO
    - Duration of therapy (hours) x low/ mean/high University HealthSystem Consortium contract pricing
  - Patient Cost of iNO
  - Duration of therapy (hours) per patient x low/mean/high University HealthSystem Consortium contract pricing
- Total Cost of iEPO
- Quantity of therapy used (bags) x AWP non-contract generic epoprostenol pricing Patient Cost of iEPO
  - Quantity of therapy used (bags) per patient x AWP non-contract generic epoprostenol pricing

#### Statistical analysis

- Categorical and continuous variables were compared by using the Student t test, x<sup>2</sup>, and the Mann-Whitney U test where appropriate All p values were two tailed and
- statistically significant at an alpha of ≤ 0.05
  - Transplant\*\* Acute RV Failure\*\*
    - ™een±SD ™een±SD ™n(%)



	Inhaled Nitris Oxide (N=53)	Inha le d Epopros te nol (N=52)	p value
Ouration of Study	3.5 ± 2.7*	3.2 ± 2.8*	0.66
Therapy, days	2.3 (0.6-4.8)†	2.0 (0.9-4.3)†	0.63
Amount of Study Therapy Used,	83.3 ± 90.0*	727 ± 85.4*	0.54
hrs	54.4 (15-115.5)†	47.9 (20.9-102.6)†	0.63

	iNO (N=53)	iEPO (¥=52)	
Total Cost, USO*			
Low IN O Contract Price Mean IN O Contract Price High INO Contract Price	206,945 486,775 749,190	43,995	<0.0001 <0.0001 <0.0001
Cost of Therapy Per Patient, USO*			
Low INO Con tact Price Mean INO Con tact Price High IN O Contract Price	3,930 ± 4,210 9,250 ± 9,910 14,240 ± 15,255	838 ± 9.97	<0.0001 <0.0001 <0.0001 <0.0001



#### Limitations

 Single center study, retrospective study

VE EI EI

- Small population size
- Change in practice

HARVARD

MEDICAL

SCHOOL

TEACHING

#### Conclusion

 Our inhaled epoprostenol requires a multidisciplinary effort from order entry to administration

Inhaled nitric oxide is 45-17 times more expensive per patient than inhaled epoprostenol

### D is clos ures

The authors of this presentation have no disclosures concerning possible financial or personal relationships with commercial entities that may have a direct or indirectinterest in the subject matter of this one sente tion

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- Khan TA, Schnickel G, Ross D, et al. A prospective, randomized, crossover pilot study of inhaled nitric coide versus inhaled prostacyclin in heart transplant and lung transplant recipients. J Thorac Cardiovasc Surg. 2009;138(6):1417-1424.
- Fiser SM, Cope JT, Kron IL, etal. Aerosolized prostacyclin (epoprostenol) as an alternative to in haled nitric oxide for patients with reperfusion injury after lung transplantion . J Thorac Cardiova.sc Surg. 2001;121:981-982.

Results

Duration of Study	3.5±2.7*	
Therapy, days	2.3 (0.6-4.8)†	1
Amount of Study Therapy Used,	83.3 ± 90.0*	
hrs brs	54.4 (15-115.5)†	47.9
† Median (IQR) Mean±SD		

	Cost				
p value		iNO (N=53)	iEPO (₩=52)		
0.21	Total Cost, USO*			-	
0.91	Low IN O Contract Price Mean IN O Contract Price High INO Contract Price	206,945 486,775 749,190	43 ,995		
0.74	Cost of Therapy Per Patient, USD*				
0.66 0.98 0.57	Low INO Con tract Price Mean INO Con tract Price High IN O Contract Price	3.930 ± 4.210 9.250 ± 9.910 1 4.240 ± 15.255	838 ± 9.97	10 N N	
0.69	USD = U.S. Dollar "Based off University Healths" contractoricing range	System Consortiu mi()	UHC) survey o	đn	
0.94					

## RESEARCH



**Open Access** 

# Nebulized heparin is associated with fewer days of mechanical ventilation in critically ill patients: a randomized controlled trial

Barry Dixon<sup>1\*</sup>, Marcus J Schultz<sup>2</sup>, Roger Smith<sup>1</sup>, James B Fink<sup>3</sup>, John D Santamaria<sup>1</sup>, Duncan J Campbell<sup>4,5</sup>

### Abstract

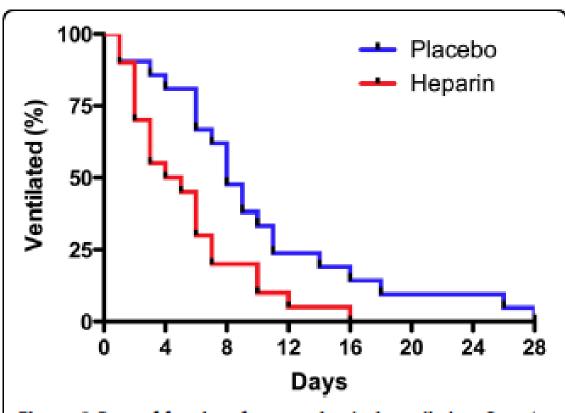
**Introduction:** Prolonged mechanical ventilation has the potential to aggravate or initiate pulmonary inflammation and cause lung damage through fibrin deposition. Heparin may reduce pulmonary inflammation and fibrin deposition. We therefore assessed whether nebulized heparin improved lung function in patients expected to require prolonged mechanical ventilation.

**Methods:** Fifty patients expected to require mechanical ventilation for more than 48 hours were enrolled in a double-blind randomized placebo-controlled trial of nebulized heparin (25,000 U) or placebo (normal saline) 4 or 6 hourly, depending on patient height. The study drug was continued while the patient remained ventilated to a maximum of 14 days from randomization.

**Results:** Nebulized heparin was not associated with a significant improvement in the primary end-point, the average daily partial pressure of oxygen to inspired fraction of oxygen ratio while mechanically ventilated, but was associated with improvement in the secondary end-point, ventilator-free days amongst survivors at day 28 (22.6  $\pm$  4.0 versus 18.0  $\pm$  7.1, treatment difference 4.6 days, 95% Cl 0.9 to 8.3, *P* = 0.02). Heparin administration was not associated with any increase in adverse events.

**Conclusions:** Nebulized heparin was associated with fewer days of mechanical ventilation in critically ill patients expected to require prolonged mechanical ventilation. Further trials are required to confirm these findings.

Trial registration: The Australian Clinical Trials Registry (ACTR-12608000121369).



**Figure 3 Rate of freedom from mechanical ventilation**. Over the first 28 days among surviving patients, the rate of freedom from mechanical ventilation was higher in patients administered heparin. Median times of ventilation were 5 days in the heparin group (n = 20) and 8 days in the placebo group (n = 21) (P = 0.01) (log-rank test).

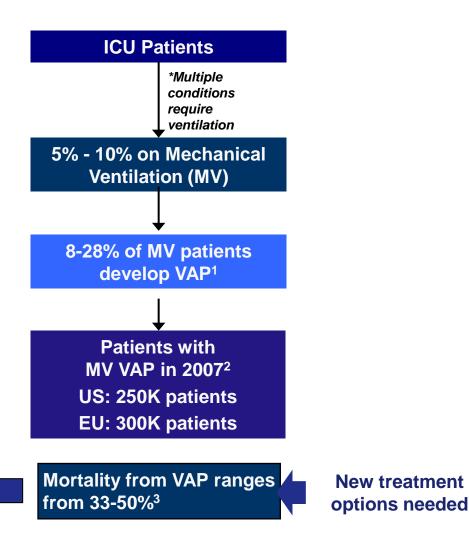
# Ventilator and Hospital Acquired Pneumonias (VAP/HAP) (MRSA)

## **Prevalence of pneumonia** high in ventilated patients



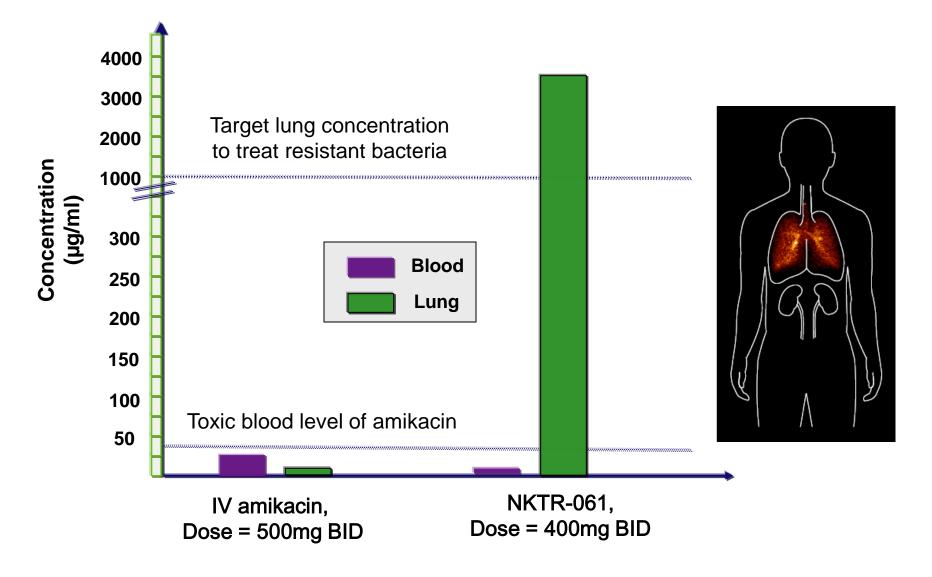
Up to 250K Deaths per year



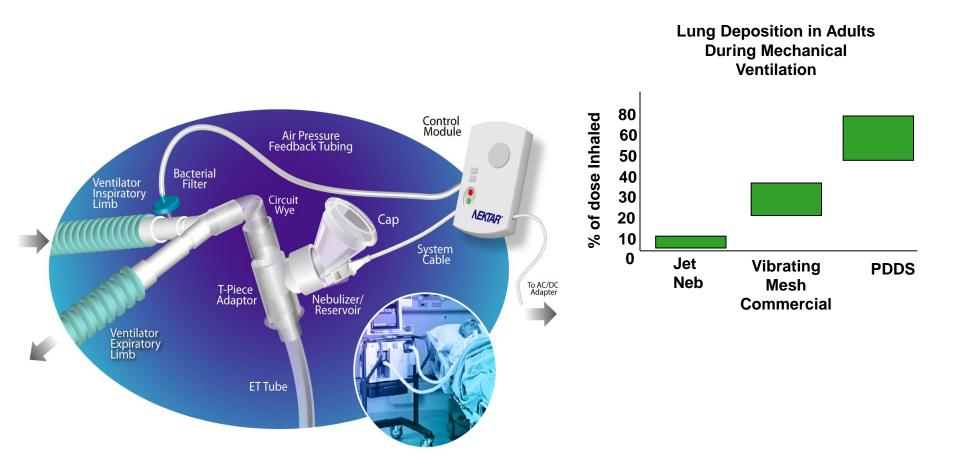


Note: \*Acute Lung Injury, Acute Respiratory, Acidosis, Apnea, Chronic Obstructive Pulmonary Disease, Hypotension, Hypoxemia, Tachypnea Source: <sup>1.3</sup> Chastre, Fagon, Am, Journal Critical Care Medicine, 2002, <sup>2</sup> AMR, <sup>4</sup> Rello, et al. Chest 2002

# Delivery of inhaled amikacin during mechanical ventilation targets the lung without systemic toxicity



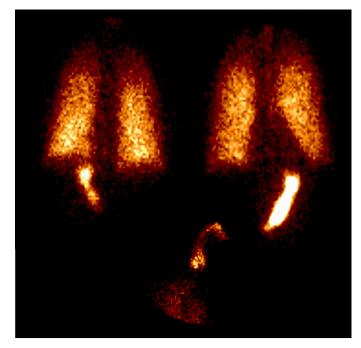
# Pulmonary Drug Delivery System for Drug Development



# Invitro/ Invivo Correlation of Inhaled Amikacin During CMV with Jet Neb, Vibrating Mesh and PDDS

	Lung Dose	Sputum Conc	Amikacin
	In Vitro %	(µg/mL/mg)	Excretion/Dose
Jet Neb	7 ± 1	6.5 ± 9.5	1.9 ±1.2
Mesh	31± 4	31 ± 35	3.8 ± 1.6
PDDS	51± 11	54 ± 71	6.4 ±2

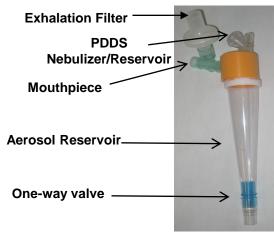
# Gamma scintigraphy study with inhaled amikacin off ventilator



Posterior and anterior scintigraphic images

In-Vitro: ED =  $87\pm2\%$ MMAD =  $3.8 \ \mu m$ 

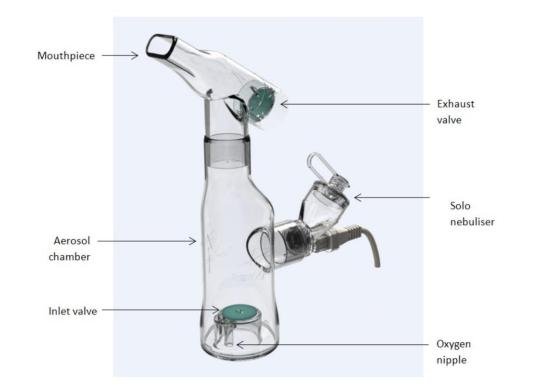
	Deposition	
	Mean	S.D.
Device	16.1	4.8
Oral	29.4	7.3
Lung	43.0	6.1
Exhaled	11.5	5.5



Hand-Held PDDS Nebulizer

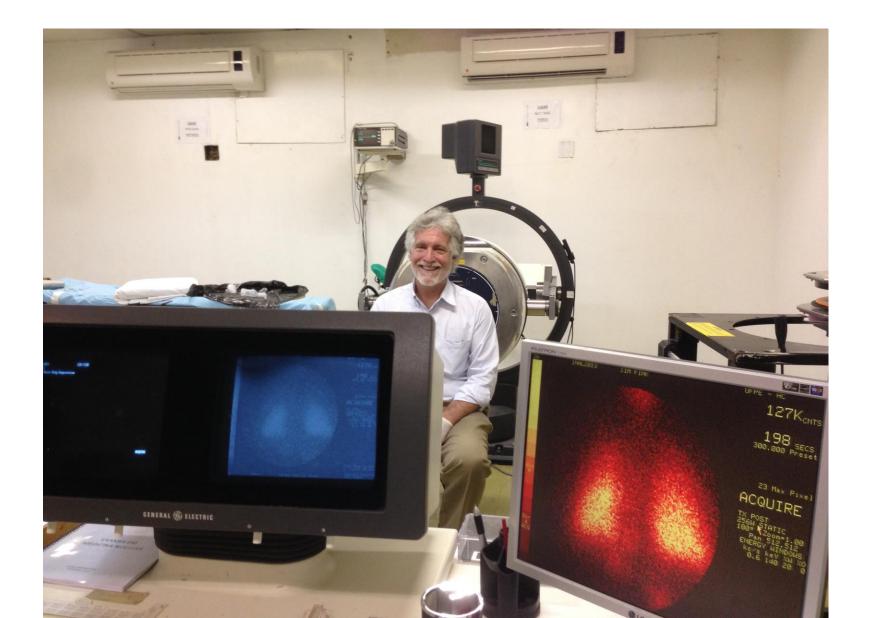
Fink J et al: In-vitro in-vivo comparison of inhaled aerosol from a hand-held nebulizer for administration of amikacin. Presented at ISAM, Tours, FR, 2007.

# Aeroneb Solo Off Vent AdaptER



O2 L/min	Mouthpiece	Open Facemask	Valved Facemask
0	71.7 ± 1.1	$1.9 \pm 0.4$	$49.6 \pm 0.9$
2	$62.4 \pm 1.3$	$49.5 \pm 2.7$	$64.2 \pm 1.9$
4	$59.3 \pm 0.5$	$45.5 \pm 4.4$	$57.1 \pm 1.5$

# Scintigraphy with Solo with Adapter



# Deposition Distribution Solo with Adapter using valved Mouthpiece

Emitted Dose	31.35
Lung Deposition	16.1-21%
Head	8.93
Stomach	1.48
Neb	11.92
Reservoir	53.93
Expiratory Filter	9.56

# Conclusion

Over the last decade aerosol delivery has changed in the ICU and Acute Care

Neonates, infants, children and adults can all get >10% lung dose with conventional ventilation.

Developments underway to approve aerosols for acute and critical care

Choice of aerosol generator and placement makes a huge difference.

Respiratory Therapist need to know so they can guide and educate the team



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